# Persistent Homology in Time Series Analysis and its Application to Wheeze Detection

Presenter: Yifan Wu Advisor: Yifei Zhu

# Content

- 1. Dynamical Systems
  - 1. Dynamical systems
  - 2. Taken's Theorem and Sliding Window Embedding
- 2. Persistent Homology
  - 1. Rips Complex
  - 2. Persistent Homology
- 3. Application to Wheeze Detection
  - 3.1. Selecting Time Delay
  - 3.2. Wheeze Modeling
  - 3.3. Experimental Results

#### References

[1] Perea, Jose A. "Topological time series analysis." *Notices of the American Mathematical Society* 66.5 (2019).

[2] Emrani Saba, Thanos Gentimis, and Hamid Krim. "Persistent homology of delay embeddings and its application to wheeze detection." *IEEE Signal Processing Letters* 21.4 (2014): 459-463.

[3] Homs-Corbera, Antoni, et al. "Time-frequency detection and analysis of wheezes during forced exhalation." IEEE Transactions on Biomedical Engineering 51.1 (2004): 182-186.

[4] Taplidou, Styliani A., and Leontios J. Hadjileontiadis. "Wheeze detection based on time-frequency analysis of breath sounds." Computers in biology and medicine 37.8 (2007): 1073-1083.

[5] Brown, Kenneth A., and Kevin P. Knudson. "Nonlinear statistics of human speech data." International Journal of Bifurcation and Chaos 19.07 (2009): 2307-2319.

- A *global continuous time dynamical system* is a pair  $(M, \Phi)$ , where *M* is a topological space and  $\Phi : \mathbb{R} \times M \to M$  is a continuous map so that  $\Phi(0, p) = p$ , and  $\Phi(s, \Phi(t, p)) = \Phi(s + t, p)$  for all  $p \in M$  and all  $t, s \in \mathbb{R}$ .
- $\mathbb{T}^2 = (\mathbb{R}/\mathbb{Z})^2$  and  $\Phi(t, (a, b)) = (a + t, b + \alpha t)$ . If  $\alpha$  is rational, then every orbit is periodic. Otherwise every orbit is dense in  $\mathbb{T}^2$ .
- A solution to an differential equation is a dynamical system, for instance:

$$x'(t) = \sigma \cdot (y - x)$$
$$y'(t) = x \cdot (\rho - z) - y$$
$$z'(t) = xy - \beta z$$

- A subset *A* ⊂ *M* called *attractor* is especially important since it attracts the evolution of states in close proximity.
- A is compact.
- *A* is an *invariant* set, i.e.  $\Phi(t, A) \subset A$  for  $t \ge 0$ .
- There is an invariant open neighborhood *U* (called *the basin of attraction*) of *A*, so that:

$$\bigcap_{t\geq 0} \Phi(t,U) = A.$$

- $\mathbb{T}^2$  is the attractor of itself if  $\alpha$  is irrational in the previous example.
- Lorenz's butterfly attractor.



- The shape of an attractor is crucial.
  - Circle implies periodic process.
  - ➢ Non-integral Hausdorff dimension implies chaos.
  - > High-dimensional tori  $\mathbb{T}^n$  implies quasiperiodicity.

- It is difficult to achieve this goal for some reasons.
  ➤ There is no precise description for the state space *M*.
  - ➤ How to figure out the "shape"?

#### Taken's Theorem

- Weather may be regarded as a dynamical system, but one can not give a precise description about it. Instead, one can easily obtain measurements of relevant quantities for each state *p* ∈ *M*, for instance temperature, pressure, etc.
- A way of measuring can be thought of as a continuous map
  *F*: *M* → ℝ called an *observation function*. For a given initial state *p* ∈ *M*, one obtains the scalar time series

 $\varphi_p: \mathbb{R} \to \mathbb{R},$  $t \mapsto F \circ \Phi(t, p).$ 

#### Taken's Theorem

• Let *M* be a smooth, compact, Riemann manifold; let  $\tau > 0$  be a real number; and let  $d \ge 2\dim(M)$  be an integer. Then for generic  $\Phi \in C^2(\mathbb{R} \times M, M)$  and  $F \in C^2(M, \mathbb{R})$ , and for  $\varphi_p(t)$ defined above, the delay map  $\psi : M \longrightarrow \mathbb{R}^{d+1}$ 

$$p \mapsto (\varphi_p(0), \varphi_p(\tau), \varphi_p(2\tau), \dots, \varphi_p(d\tau))$$

is an embedding.

• Generic means that  $\Phi$ , *F* are both open and dense in Whitney topology.

## Sliding Window Embedding

Let *f* : ℝ → ℝ be a function, τ > 0 a real number, and *d* > 0 an integer. The *sliding window embedding* of *f*, with paremeters *d* and τ, is the vector valued function

$$SW_{d,\tau}f: \mathbb{R} \to \mathbb{R}^{d+1},$$

$$t\mapsto (f(t),f(t+\tau),f(t+2\tau),\ldots,f(t+d\tau)).$$

• For  $T \subset \mathbb{R}$ , the set  $\mathbb{SW}_{d,\tau}f = \{SW_{d,\tau}f(t): t \in T\}$  is the *sliding window point cloud* associated to the *sampling set T*.

# Sliding Window Embedding

- Thus, given time series data  $f(t) = \varphi_p(t)$  observed from a potentially unknown dynamical system  $(M, \Phi)$ , Taken's theorem implies that the sliding window point cloud  $SW_{d,\tau}f$  provides a topological copy of  $\{\Phi(t, p): t \in T\}$ .
- Therefore, one successfully carries the orbit of a point *p* ∈ *M* homeomorphically to an Euclidean space!

# Rips Complex

For a finite set of points X = {x<sub>i</sub>}, we can form a simplicial complex (abstract) called *Rips complex* R<sub>α</sub>(X):

$$\mathcal{R}_{\alpha}(\mathcal{X}) = \left\{ \left\{ x_{i_1}, \cdots, x_{i_k} \right\} \subset \mathcal{X} : d\left( x_{i_p}, x_{i_q} \right) \le \alpha, 0 \le p, q \le k \right\}.$$



# Rips Complex

- Let H<sub>n</sub>(R<sub>α</sub>(X); F) denote the n'th homology group (vector space) of Rips complex of X with coefficients in filed F, usually F<sub>2</sub>. Let β<sub>n</sub>(R<sub>α</sub>(X); F) denote the rank (dimension) of H<sub>n</sub>(R<sub>α</sub>(X); F), called the *n'th Betti number* of R<sub>α</sub>(X). Betti number implies the number of n-dimensional holes in a given topological space.
- If  $\alpha \leq \alpha'$ , there is an inclusion  $\iota^{\alpha,\alpha'}$  from  $\mathcal{R}_{\alpha}(\mathcal{X})$  to  $\mathcal{R}_{\alpha'}(\mathcal{X})$ ,  $\iota^{\alpha,\alpha'}(\{x_{i_1},\cdots,x_{i_k}\}) = \{x_{i_1},\cdots,x_{i_k}\},\$

and induces a linear transformation:

$$\iota_n^{\alpha,\alpha'}: H_n(\mathcal{R}_{\alpha}(\mathcal{X}); \mathbb{F}) \longrightarrow H_n(\mathcal{R}_{\alpha'}(\mathcal{X}); \mathbb{F}).$$

- A *persistence vector space*  $\mathbb{V}$  is a collection of vector spaces  $V_{\alpha}, \alpha \in \mathbb{R}$ , and linear transformations  $\iota^{\alpha,\alpha'}: V_{\alpha} \to V_{\alpha'}, \alpha \leq \alpha'$ , so that:
- 1.  $\iota^{\alpha,\alpha}$  is the identity map of  $V_{\alpha}$  for all  $\alpha$ .
- 2.  $\iota^{\alpha',\alpha''} \circ \iota^{\alpha,\alpha'} = \iota^{\alpha,\alpha''}$  for all  $\alpha \le \alpha' \le \alpha''$ .
- If  $\gamma \in V_{\alpha}$  is a nonzero element, then define  $birth(\gamma) = \inf \{ \tilde{\alpha} \le \alpha : \gamma \in \operatorname{Im}(\iota^{\tilde{\alpha},\alpha}) \}$   $death(\gamma) = \sup \{ \alpha' \ge \alpha : \gamma \notin \operatorname{Ker}(\iota^{\alpha,\alpha'}) \}$  $persistence(\gamma) = death(\gamma) - birth(\gamma)$

• We will use  $bcd_n^{\mathcal{R}}(\mathcal{X}; \mathbb{F})$  to denote the barcode for the n-dimensional persistent homology of  $\mathcal{R}(\mathcal{X})$ .



Figure 1.[Perea, 2019] Barcode for the Rips filtration of  $\mathcal{X} \subset \mathbb{R}^2$  near  $S^1$ .

- Let V be a persistence vector space so that dim(V<sub>α</sub>) is finite for all α. Then there exists a multiset of intervals *I* called the barcode of V, denoted *bcd*(V), and so that:
- 1. For all  $\alpha$ , dim( $V_{\alpha}$ ) is exactly the number of intervals  $I \in bcd(\mathbb{V})$ , counted with repetitions, with  $\alpha \in I$ .
- 2. For every  $I \in bcd(\mathbb{V})$ , and  $\alpha \in I$ , there is  $\gamma \in V_{\alpha}$  with the left and right end-points of *I* are  $birth(\gamma)$  and  $death(\gamma)$ .
- $H_n(\mathcal{R}_\alpha(\mathcal{X}); \mathbb{F})$  together with maps  $\iota_n^{\alpha, \alpha'}$  is a persistence vector space, called the *n*-dimensional persistent homology, with coefficients in  $\mathbb{F}$ , of the *Rips filtration*  $\mathcal{R}(\mathcal{X}) = \{\mathcal{R}_\alpha(\mathcal{X})\}_{\alpha \in \mathbb{R}}$ .

• Let  $\omega = \sqrt{3}$  be irrational. Consider the dynamics  $\Phi$  and observation function *F* on torus  $\mathbb{T}^2 = S^1 \times S^1 \subset \mathbb{C}^2$ , given by

$$\Phi: (t,(z_1,z_2)) \to (e^{it}z_1,e^{i\omega t}z_2)$$

$$F:(z_1,z_2) \longrightarrow \operatorname{Re}(z_1+z_2).$$

Let 
$$p = (1,1), d = 4, \tau = \frac{3}{4}\sqrt{3}\pi, n = 0,1,2.$$



Figure 2.[Perea, 2019] Left: The orbit of point p. The colors, blue through red, indicate the time. Center: The time series  $f(t) = F \circ \Phi(t, p) = \cos t + \cos \sqrt{3}t$ . Right: Barcodes for the Rips filtration  $\mathcal{R}(\mathbb{SW}_{d,\tau}f)$ , the number of long intervals recovers the Betti numbers of the orbit:  $\beta_0 = \beta_2 = 1$ ;  $\beta_1 = 2$ .

#### Application to Wheeze Detection

• For a scalar time series {*x<sub>i</sub>*}, a representation of the delay coordinate embedding can be described as the following vector quantity of *m* components:

$$X_i = (x_i, x_{i+j}, x_{i+2j}, \dots, x_{i+(m-1)j})$$

Where *j* is the index delay and *m* is the embedding dimension. If the sampling time is  $T_s$ , then the delay time  $\tau$  is connected to the index delay *j* by the equality  $\tau = j \cdot T_s$ . We will use *m* = 2 in the rest of our discussion.

• Discrete time sound signals can be considered as a series expressing the amplitude of the wave in volts at each time instance, i.e.  $x(t_i) = x_i$ , i=1,2,...k and  $t_i = i \cdot T_s$ .

# Application to Wheeze Detection

- Taken's theorem implies that this embedding carries the whole topological data.
- Thus for a given discrete time sound signal  $x(t_i)$ , we can embed it into  $\mathbb{R}^2$ , then use the proposed persistent homology method to suggest the shape of the original signal.
- There are still something to be done, namely, selecting time delay and wheeze modeling.

# Selecting Time Delay

• Examine an autocorrelation-like function(ACL) to choose a proper delay. The ACL function of a non-stationary digital signal  $x(t_i)$  is calculated as follows:

$$R_{xx}(t_i) = \sum_{1 \le l \le k} x(t_i) \cdot x(t_l)$$

• According to experimental results, the appropriate interval for choosing delay time is  $t_{c1} < \tau < t_{c2}$ , where  $t_{c1}$  and  $t_{c2}$  are the first and second critical points of the ACL function  $R_{xx}(t_i)$ .

## Selecting Time Delay



Figure 3.[Emrani Saba, 2014] The ACL function of a non-wheeze signal (left) and a wheeze signal (right).

• We propose a model for wheeze signals in time domain defined as a continuous piecewise sinusodal function with different periods and phases and a time varying amplitude, represented as

$$\omega(t) = \sum_{i=1}^{n} g_i(t)$$

$$g_i(t) = \begin{cases} A(t) \sin\left(\frac{2\pi}{T_i}t + \phi_i\right), t_{i-1} \le t \le t_i \\ 0 \end{cases}$$

• For each discrete wheeze signal denote by s(t), we can construct such a  $\omega(t)$ .

• This model performs well on wheeze signals but not good on non-wheeze signals.



Figure 4.[Emrani Saba, 2014] Comparison of the proposed model for a nonwheeze breathing sound signal (left) and a wheeze signal (right).

Now we turn to embed ω(t) and apply our method. To be precise, the continuous time delay embedding of ω(t) and ω<sub>i</sub>(t) can be defined as:

$$W(t) = \left\{ \left( \omega(t), \omega(t+\tau) \right) : t \in \mathbb{R} \right\}$$
$$W_i(t) = \left\{ \left( \omega_i(t), \omega_i(t+\tau) \right) : t_{i-1} \le t \le t_i \right\}$$

• Lemma : The time delay embedding of a sinusoidal function with a suitable time delay is an ellipse.

- The time delay embedding W of a wheeze signal is similar to the union of  $W_i$  with few point missed. And therefore, the Rips complex associated to the corresponding point cloud of W is close to a set of concentric ellipse with angles of rotation  $\pm 45^\circ$ , which always has at least one 1-dimensional persistent hole.
- On the other hand, using experimental results, the one shows that the first persistent Betti number of the delay embedding of a non-wheeze signal is zero.

#### 3.3. Experimental Results

![](_page_26_Figure_1.jpeg)

Figure 5.[Emrani Saba, 2014] Delay-embedding of non-wheeze signals recorded over (a) apex, (b) midlung and (c) chest. Delay embeddings of some wheeze signals.

#### 3.3. Experimental Results

![](_page_27_Figure_1.jpeg)

Figure 6.[Emrani Saba, 2014] Point cloud sampling, (a) and (d): the delay embedding of a non-wheeze and a wheeze signal including 4000 points, 100 subsamples slected using random method (b)(e) and maximin method (c)(f).

![](_page_28_Figure_0.jpeg)

Figure 7.[Emrani Saba, 2014] The barcodes for a non-wheeze breathing sound signal (left) and a wheeze signal (right). The "significant" barcode is highlighted in red and is used to distinguish wheeze signals from non-wheeze signals.

#### 3.3. Experimental Results

• The accuracy of proposed technique is 98.39% while the accuracy of the time-frequency analysis techniques proposed in [3] and [4] without using persistent homology are 86.2% and 95.5%, respectively.

# Thanks!